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(19) (CA) **APPLICATION FOR CANADIAN PATENT** (12)

(54) Articulated Stent

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ABSTRACT

In a first embodiment a number of stent segments are connected together by hinges welded in place to provide articulation between the stent segments. The hinges can be, among other shapes, either a straight wire or a coiled wire of biocompatible material. A second embodiment uses a stent of a previous invention made up of a number of wires welded together for the stent segments with connection between adjacent stents provided by having one of the wires of adjacent stents continue between these adjacent stents to provide a hinge action. In this embodiment the wire portion extending between the segments is ground to a smaller diameter than the wire of the stent segment itself, to provide the necessary hinge flexibility. This articulated stent, made up of a number of individual stent segments, gives support for curved arteries, with the hinges between the segments providing both articulation and spacing between the stent segments. This articulated stent is tailored to match the curvature existing in the artery and is positioned at the site with the necessary preferred angular orientation using a previous catheter system.

ARTICULATED STENT

Field of the Invention

5 The present invention relates to
intravascular stents which are applied within
the peripheral or coronary arteries of a living
10 animal or human being to maintain patency after
a balloon angioplasty, either a percutaneous
transluminal coronary angioplasty (PTCA) or a
percutaneous transluminal angioplasty (PTA)
procedure. This invention relates particularly
15 to arteries which have a curved portion, curved
and recurved portions, changes in diameter,
which are difficult to obtain using existing
stents; and also to extend the length of
coverage provided by a single stent which can
20 be installed during a single procedure.

Background of the Invention

 The advantage of utilizing a stent in
conjunction with a PTCA or PTA procedure is
well known. Earlier stents required an
20 expansion procedure to expand the stent to
provide support for the blood vessel after
implantation. Later improvements including
U.S. Pat. 4,830,003 regarding a Compressive
Stent and Delivery System, Rodney G. Wolff et
25 al co-invented by me, utilized a catheter
system to hold a spring loaded stent compressed
and to place the stent at the desired location

within an artery. This approach greatly improved the utility of the stent and minimized previous problems, but required the use of multiple stents to provide support where a blood vessel curved to any extent and for extended lengths. While such an approach is possible the difficulty of spacing separate adjoining stents accurately and possible interference between these adjacent stents can reduce their effectiveness and will always increase the procedure time.

Summary of the Invention

The problems associated with the use of multiple stents in curved arteries, or arteries having a change in size such as at a branch, led to my developing the instant device. This device utilizes a number of stent segments flexibly connected together by a hinge between each adjacent stent segment. This approach not only allows use of unequal diameter stent segments as the artery diameter changes, and permits articulation between adjacent stent segments, but also maintains the spacing between adjacent segments as established by the hinge lengths. In a first embodiment my prior co-invention, which utilizes a stent made up of a number of individual wires welded into a tubular shaped structure for the stent segments, is incorporated as an example. This use of my previous stent is merely illustrative

here as any metal stent segments can be connected together using a metal hinge welded between adjoining stent segments. A relatively small number of stent segments are shown in the example but as many segments as may be required can be attached together using this approach. When the stent is located within an artery which has a bend, the hinges are preferably located on the outside of the bend. This permits the hinge to provide additional support between stent segments on the outside of the bend and also permits the inside edge of the stent to close to provide additional support on that side. It follows that where an artery curves in only one direction, all of the hinges will be located on one side. In cases where an artery curves first in one direction and then in the opposite direction however, the first hinge will be located on one side and the second hinge on the opposite side to provide the required matching stent articulation. Likewise any other angular relationship can be accommodated by the appropriate location of the hinges in relation to the stent circumference of adjacent stent segments.

For all applications the artery size and shape is measured first to determine the number of stent segments, their respective diameters, lengths, stent segment spacing, and the support required of each respective stent segment. The

5 hinge characteristics as to length, strength
and location on the stent circumference are
also determined from these measurements. An
articulated stent is then manufactured to
conform to this specific artery by
incorporating all of the respective stent and
hinge requirements into this stent. The
catheter system of my previous co-invention is
also utilized here to deliver this articulated
10 stent to the arterial site with the proper
orientation. The hinges are made either of
radiopaque material or are coated with
radiopaque material to permit observation of
the angular orientation of the stent relative
15 to the blood vessel. Rotating the appropriate
catheter will rotate the articulated stent to
the correct orientation aided by simultaneously
observing the results on a fluoroscope during
the rotation. This rotation is accomplished
20 after the stent is positioned at the site. The
prior site positioning and placement using this
previous catheter system are employed
essentially the same here as for my previous
single segment stent.

25 The hinge used can be simply a wire welded
between adjacent stent segments. Where
additional flexibility for a given hinge
strength is needed, the wire hinge can be
coiled along its length in a manner similar to
30 a coiled lamp filament. This approach retains

the strength of a particular wire size but provides much greater flexibility between stent segments. Any other metal shape having the necessary hinge characteristics can be used for this hinge segment however.

While this hinge works well with my previously co-invented wire stent there is no limitation in this approach which requires that it be used with only my stent. Further, any kind of metallic stent can be welded to a metal hinge by using either laser or resistance welding.

A second embodiment, which requires the use of my previous stent, provides the hinges by extending one of the wires making up adjacent stent segments continuously both through the stents and also through the gap between them. This continuous wire is normally not the same gage between the stent segments as the wires in the stent segments themselves. This wire is usually ground to a smaller diameter in the spaces between the stents to provide additional flexibility for the hinge function. This continuous wire provides the necessary hinge action between the stent segments rather than welding a separate hinge in place.

As before, when an artery is curved in one direction only, the continuous wire can extend through and between all stent segments. When

the artery curves change direction, then the continuous wires preferably extend only through contiguous segments which are bent in the same direction. For example, where a first bend in one direction is followed by a second bend in an opposite direction, a first continuous wire will extend only through a first and second segment and the gap between them on one side of the articulated stent, and a second continuous wire will extend only through the second and a third segment and the gap between them on the opposite side. This change in direction is accommodated by this change in
10 the location of the continuous wire which extends between subsequent stent segments relative to the stent circumference. Any change in direction of subsequent bends can be accommodated by extending the wire on the appropriate side between segments.

According to a broad aspect of the invention there is provided an articulated stent comprising:

(a) at least two segments made up of stent means having an axial bore therethrough and made of metal;

(b) flexible hinge means formed of biocompatible metal attached to said stent means, and arranged such as to flexibly
20 connect said segments together with the axial bores of adjacent stent means generally aligned.

According to another broad aspect of the invention there is provided an articulated stent having at least two segments made up of stents of the type having a number of wires welded together and formed into a generally tubular shape, the improvement comprising having a wire of each pair of adjoining segments

common to both segments such that a portion of the common wire extending between adjoining stent segments provides a hinge function.

Description of the Drawings

Figure 1 shows an articulated stent of three stent segments connected together by two wire hinges welded to the same side of the segments.

Figure 2 shows the articulated stent of Figure 1 in situ in an artery which has a bend in one direction only.

10

Figure 3 shows an articulated stent of three wire segments connected together by two coiled wire hinges welded in place.

FIG. 4 shows an articulated stent of three stent segments connected together by two wires extending between and through the opposite sides of adjoining stent segments.

5 FIG. 5 shows the articulated stent of FIG. 4 in situ in an artery shown in cross-section which has bends in two directions.

10 FIG. 6 shows an articulated stent with segments of unequal size joined by a welded wire hinge.

FIG. 7 is a detail of a hinge welded to the end of two adjacent stent segments.

15 FIG. 8 is a detail of the stent delivery system of my previous co-invention in an artery in cross-section, holding an articulated stent.

FIG. 9 shows the catheters and guide wires of my previous co-invention delivery system.

Detailed Description of the Preferred Embodiments

20 In FIG. 1 an articulated stent 10 is shown with three stent segments 12 and two interconnecting hinges 14. Stent segments 12 are each made of individual wire elements welded together, as described in my previous co-invention. Hinges 14 are made of
25 biocompatible spring material and are of a smaller diameter than those used in forming stent segments 12. Hinges 14 are welded at each end to stent segments 12 using either laser or resistance welding techniques. Hinges
30 14 are both attached to the same side of stent

segments 12. This is because stent 10, shown
in FIG. 1, is installed in artery 16, as shown
in FIG. 2 which bends in one direction only.
Hinges 14 are all located on the outside of the
5 bend with the inner edges of stent segments 12
closer together because of the bend. This
hinge location for the hinges accomplishes two
purposes. First, hinges 14 act as a bridge
between adjacent stent segments 12 to provide
10 additional support for the artery. Second,
since the edges of stent segments 12 on the
side opposite to hinges 14 are bent toward each
other, having the hinge spacing located on the
outside portion of the articulated stent 10
15 allows these inner edges to close. This also
provides additional arterial support on this
inside edge. These hinges, as discussed
earlier, can either be made of radiopaque
material or can be coated with radiopaque
20 material to permit determining the orientation
of the articulated stent within an artery using
a fluoroscope.

In use, the articulated stent is delivered
to the site using the same delivery scheme as
25 for my previous co-invention as shown in FIGS.
8 and 9; having a guide catheter 51, an outer
catheter 52 to compress and position the stent
within the blood vessel, an inner catheter 54
to hold the stent at the desired site while the
30 outer catheter is removed to deposit the stent

in situ and an optional guide wire 56. If the stent orientation is incorrect, the outer catheter 52 is rotated within the guide catheter 51 to obtain the desired orientation while observing the results on a fluoroscope screen.

In FIG. 3 articulated stent 18 is made up of three stent segments 20 which are connected together by two coiled hinges 22 consisting of a wire coiled about its length. Hinge 22 is also welded at each end to a wire of the adjacent stent segment 20. As discussed previously, coiling the wire making up hinge 22 increases the bending flexibility of the wire while retaining the strength.

In FIG. 4 an articulated stent 28 is made up of three stent segments 30 connected together by two wires 32 which extend through and are a part of the respective adjoining segments. Wires 32 are located generally on opposite sides of the articulated stent and each wire is welded to and made a part of the the adjacent stent segments 30. The diameter of wires 32 between adjacent stent segments 30 is reduced by a grinding process to provide additional flexibility in this hinge region. This opposed arrangement of wires 32, which effectively form the hinges is used when a bend and a reverse bend are adjacent to each other in an artery which must be supported by

an articulated stent, since the hinges are preferably located on the outside of the bends. In FIG. 5 articulated stent 28 of FIG. 4 is installed within an artery 34 which has such a bend and a reverse bend.

In Fig. 6 an articulated stent is shown with a stent segment 38 which is larger than another stent segment 36 which are connected by a hinge 42. This illustrates how a change in diameter of an artery can be accommodated.

In FIG. 7 a detail of a wire hinge 44 welded to the ends of two adjacent stent segments 46 is shown. A wire or any other metal segment having equivalent flexibility can be used to connect adjacent metal stent segments together to provide the necessary function.

The articulated stents shown here are only representative of some of a great number of possible combinations of stent segments. Further, any other metal stent segments which are taught elsewhere including dissimilar types of stent segments, can be attached together using the biocompatible metal hinges of this invention, by merely welding the hinges in place. The hinges can be of any type, length, or diameter.

The fact that this articulated stent can be tailored for the requirements of any arterial site is the essence of this invention.

5 The artery to be supported is mapped prior to
a PTCA or PTA procedure to determine the
required diameter, support, and spacing of each
stent segment and the flexibility and length
10 of each hinge. An articulated stent is then
manufactured taking all of these requirements
into account. After the PTCA or PTA procedure,
while the guide catheter is still in place, the
outer catheter, inner catheter, articulated
15 stent and guide wire are then placed within
the guide catheter to position the articulated
stent in situ.

While this invention has been described
with reference to illustrative embodiments,
15 these descriptions are not intended to be
construed in a limiting sense. Various
modifications of the illustrative embodiments,
as well as other embodiments of the invention,
will be apparent to persons skilled in the art
20 upon reference to this description. It is
therefore contemplated that the appended claims
will cover any such modifications or
embodiments as fall within the true scope of
the invention.

25

THE EMBODIMENTS OF THE INVENTION IN WHICH AN EXCLUSIVE
PROPERTY OR PRIVILEGE IS CLAIMED ARE DEFINED AS FOLLOWS:

- 1 1. An articulated stent comprising:
 - 2 (a) at least two segments made up
 - 3 of stent means having an axial bore there-
 - 4 through and made of metal;
 - 5 (b) flexible hinge means formed of
 - 6 biocompatible metal attached to said stent
 - 7 means, and arranged such as to flexibly connect
 - 8 said segments together with the axial bores of
 - 9 adjacent stent means generally aligned.
- 1 2. Hinge means as in claim 1 being made
- 2 of radiopaque material.
- 1 3. Hinge means as in claim 1 comprised
- 2 of a generally straight wire.
- 1 4. Hinge means as in claim 3 being made
- 2 of radiopaque material.
- 1 5. Hinge means as in claim 1 comprised
- 2 of a wire coiled about a longitudinal axis
- 3 extending between adjacent stent segments.
- 1 6. Hinge means as in claim 5 made of
- 2 radiopaque material.

1 7. An articulated stent having at least
2 two segments made up of stents of the type
3 having a number of wires welded together and
4 formed into a generally tubular shape, the
5 improvement comprising having a wire of each
6 pair of adjoining segments common to both
7 segments such that a portion of the common wire
8 extending between adjoining stent segments
9 provides a hinge function.

1 8. An articulated stent as in claim 7
2 whereby the portions of the common wires
3 between adjoining stent segments have a reduced
4 diameter.

1 9. An articulated stent as in claim 7
2 whereby the portions of the common wires
3 between adjoining stent segments are made of
4 radiopaque metal.

1 10. An articulated stent as in claim 7
2 whereby the portions of the common wires
3 between adjoining stent segments are coiled
4 about a longitudinal axis.

1 11. An articulated stent as in claim 10
2 whereby the portion of the common wires between
3 adjoining stent segments are made of radiopa-
4 que material.

SMART & BIGGAR
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PATENT AGENTS

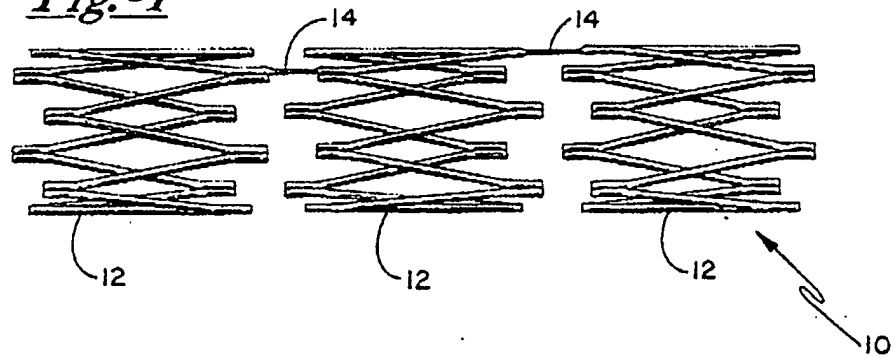
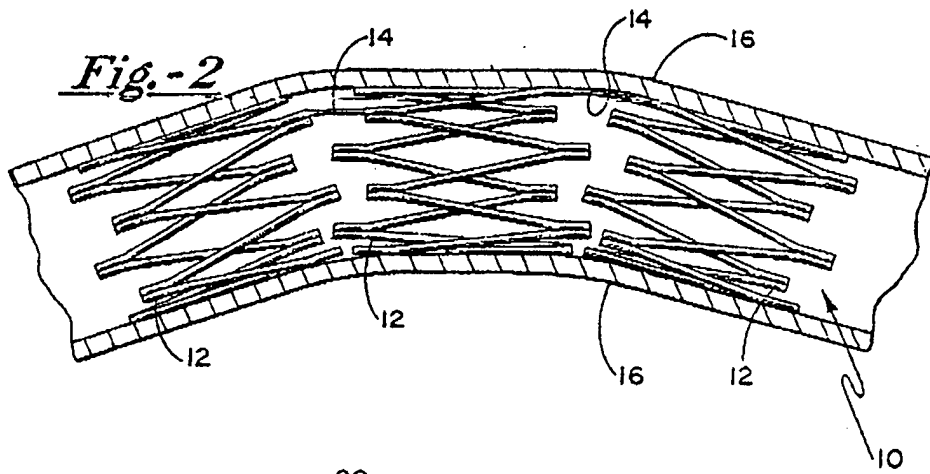
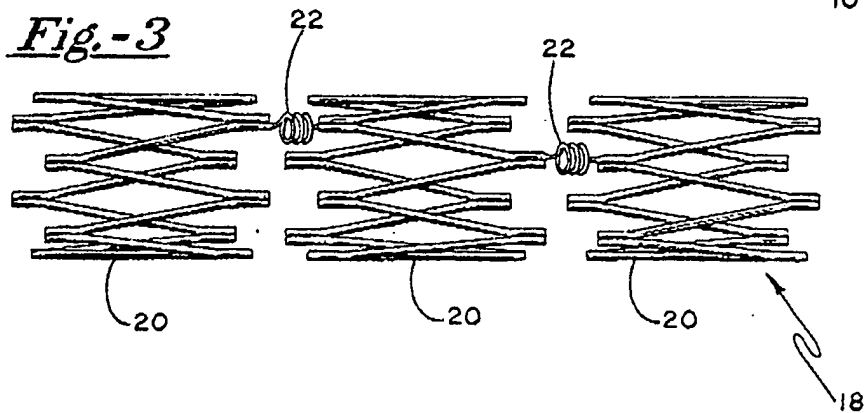
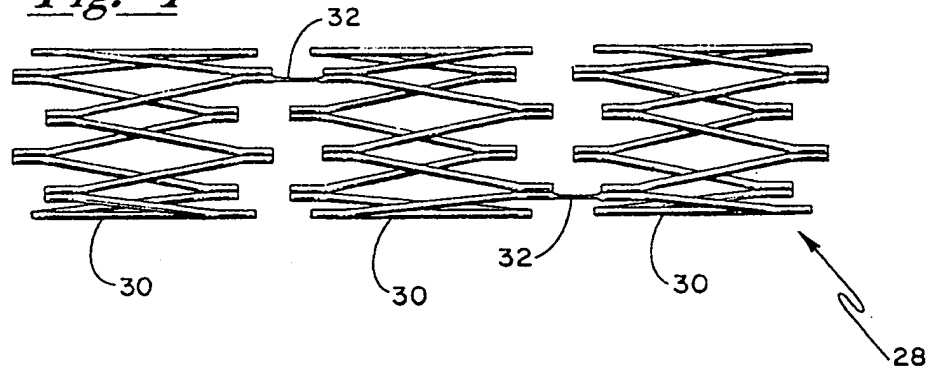
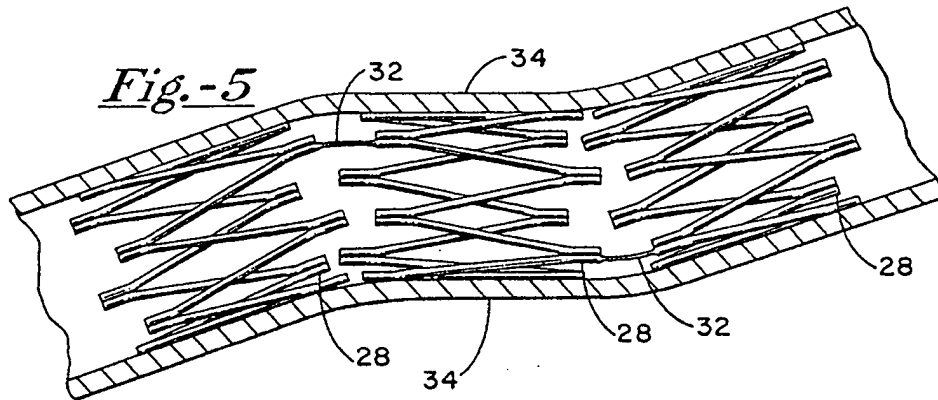
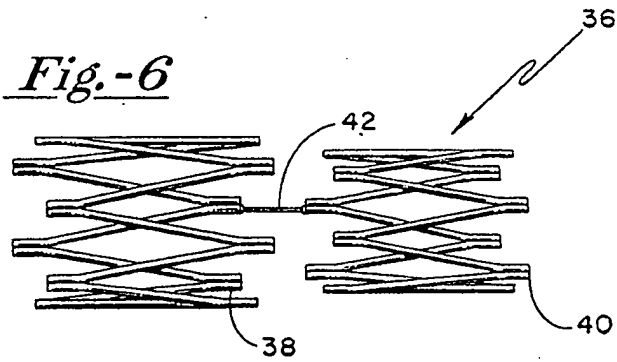
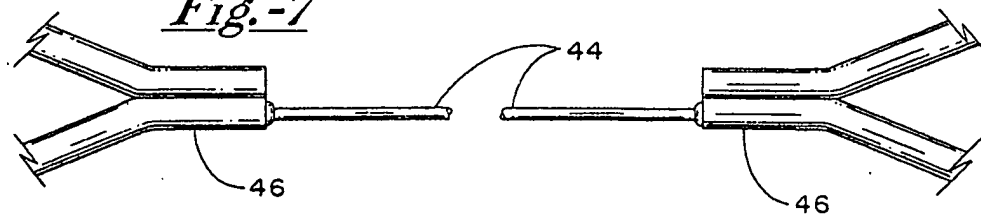
Fig.-1*Fig.-2**Fig.-3*

Fig.-4*Fig.-5**Fig.-6**Fig.-7*

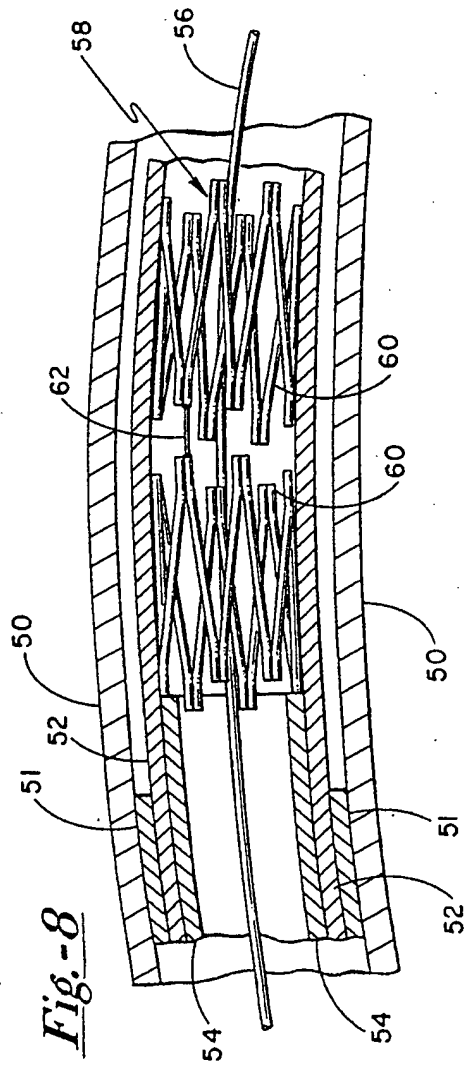


Fig.-9
PRIOR ART

